



## INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

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(54) Title: METHOD FOR PRESERVING A HEMOGLOBIN BLOOD SUBSTITUTE (54) Titre: PROCEDE DE CONSERVATION D'UN SUBSTITUT DE SANG DERIVE DE L'HEMOGLOBINE			
(57) Abstract			
<p>The present invention relates to a method for preserving a deoxygenated hemoglobin blood substitute and to a preserved deoxygenated blood substitute. The present invention is drawn to a method for preserving a deoxygenated hemoglobin blood substitute comprising maintaining the deoxygenated hemoglobin blood substitute in an oxygen barrier film primary package comprising a transparent laminate material, said film having an oxygen permeability of less than about 1.0 cc per 100 square inches (or about 0.155 cc per 100 square centimeters) per 24 hours per atmosphere at about 25°C and an external relative humidity of about 50%. The present invention is also drawn to a preserved deoxygenated hemoglobin blood substitute. Said preserved blood substitute comprises a deoxygenated hemoglobin blood substitute and an oxygen barrier film primary package. Said oxygen barrier film primary package comprises a transparent laminated material, having an oxygen permeability of less than about 1.0 cc per 100 square inches (or about 0.155 cc per 100 square centimeters) per 24 hours per atmosphere at about 25°C and an external relative humidity of about 50%, within which the deoxygenated hemoglobin blood substitute is sealed, thereby preserving the deoxygenated hemoglobin blood substitute in an environment that is substantially free of oxygen.</p>			
(57) Abrégé			
<p>La présente invention concerne un procédé de conservation d'un substitut de sang dérivé d'hémoglobine désoxygénée et un substitut de sang désoxygéné conservé selon ce procédé. Ce procédé consiste à conserver un substitut de sang tiré d'hémoglobine désoxygénée dans une enveloppe primaire faite d'un film imperméable à l'oxygène lui-même constitué par un film laminé transparent. Ce film a une perméabilité à l'oxygène inférieure à environ 1,0 cc par 100 po2ℓ (soit environ 0,155 cc par 100 cm2ℓ) par 24 heures et par atmosphère à une température d'environ 25 °C et pour une humidité extérieure relative de quelque 50 %. Cette invention concerne également un substitut de sang tiré d'hémoglobine désoxygénée ainsi conservé. Ledit substitut de sang conservé comprend un substitut de sang dérivé d'hémoglobine désoxygénée et une enveloppe primaire à film imperméable à l'oxygène. Cette enveloppe primaire est constituée par un film laminé transparent possédant une perméabilité à l'oxygène inférieure à environ 1,0 cc par 100 po2ℓ (soit environ 0,155 cc par 100 cm2ℓ) par 24 heures et par atmosphère à une température d'environ 25 °C et pour une humidité extérieure relative de quelque 50 %, dans laquelle le substitut de sang tiré d'hémoglobine désoxygénée est hermétiquement scellé, ce qui permet de le conserver dans un environnement essentiellement exempt d'oxygène.</p>			

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<p>(21) International Application Number: PCT/US99/23631</p> <p>(22) International Filing Date: 13 October 1999 (13.10.99)</p> <p>(30) Priority Data: 09/173,189 14 October 1998 (14.10.98) US</p> <p>(63) Related by Continuation (CON) or Continuation-in-Part (CIP) to Earlier Application US 09/173,189 (CON) Filed on 14 October 1998 (14.10.98)</p> <p>(71) Applicant (for all designated States except US): BIOPURE CORPORATION [US/US]; 11 Hurley Street, Cambridge, MA 02141 (US).</p> <p>(72) Inventors; and (75) Inventors/Applicants (for US only): GAWRYL, Maria, S. [US/US]; 28 Constitution Road, Charlestown, MA 02129 (US). HOUTCHENS, Robert, A. [US/US]; 22 Briar Drive, Milford, MA 01757 (US). LIGHT, William, R. [US/US]; 3 Mohegan Trail, Natick, MA 01760 (US).</p>		<p>(74) Agents: PIERCE, N., Scott et al.; Hamilton, Brook, Smith &amp; Reynolds, P.C., Two Millda Drive, Lexington, MA 02421 (US).</p> <p>(81) Designated States: AE, AL, AM, AT, AU, AZ, BA, BB, BG, BR, BY, CA, CH, CN, CR, CU, CZ, DE, DK, DM, EE, ES, FI, GB, GD, GE, GH, GM, HR, HU, ID, IL, IN, IS, JP, KE, KG, KP, KR, KZ, LC, LK, LR, LS, LT, LU, LV, MA, MD, MG, MK, MN, MW, MX, NO, NZ, PL, PT, RO, RU, SD, SE, SG, SI, SK, SL, TJ, TM, TR, TT, TZ, UA, UG, US, UZ, VN, YU, ZA, ZW, ARIPO patent (GH, GM, KE, LS, MW, SD, SL, SZ, TZ, UG, ZW), Eurasian patent (AM, AZ, BY, KG, KZ, MD, RU, TJ, TM), European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, GW, ML, MR, NE, SN, TD, TG).</p> <p><b>Published</b> <i>With international search report. Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i></p>
(54) Title: METHOD FOR PRESERVING A HEMOGLOBIN BLOOD SUBSTITUTE		
(57) Abstract		
<p>The present invention relates to a method for preserving a deoxygenated hemoglobin blood substitute and to a preserved deoxygenated blood substitute. The present invention is drawn to a method for preserving a deoxygenated hemoglobin blood substitute comprising maintaining the deoxygenated hemoglobin blood substitute in an oxygen barrier film primary package comprising a transparent laminate material, said film having an oxygen permeability of less than about 1.0 cc per 100 square inches (or about 0.155 cc per 100 square centimeters) per 24 hours per atmosphere at about 25°C and an external relative humidity of about 50%. The present invention is also drawn to a preserved deoxygenated hemoglobin blood substitute. Said preserved blood substitute comprises a deoxygenated hemoglobin blood substitute and an oxygen barrier film primary package. Said oxygen barrier film primary package comprises a transparent laminated material, having an oxygen permeability of less than about 1.0 cc per 100 square inches (or about 0.155 cc per 100 square centimeters) per 24 hours per atmosphere at about 25°C and an external relative humidity of about 50%, within which the deoxygenated hemoglobin blood substitute is sealed, thereby preserving the deoxygenated hemoglobin blood substitute in an environment that is substantially free of oxygen.</p>		

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**Description**

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## METHOD FOR PRESERVING A HEMOGLOBIN BLOOD SUBSTITUTE

## RELATED APPLICATIONS

This application is a Continuation of copending U.S. Patent Application Serial No. 09/173,189, filed October 14, 1998, which is a Continuation-in-Part of copending U.S. Patent Application Serial No. 08/974,658, filed on November 19, 1997 now abandoned, which is a Continuation of U.S. Patent Application Serial No. 08/471,583, filed June 7, 1995 now issued Patent 5,691,452, which is a Continuation-in-Part of U.S. Patent Application Serial No. 08/458,916, filed June 2, 1995 now issued Patent 5,840,852, which is a Continuation of U.S. Patent Application Serial No. 08/409,337, filed March 23, 1995 now issued Patent No. 5,854,209, the entire teachings of which are incorporated herein by reference.

## BACKGROUND OF THE INVENTION

There exists a need for a blood substitute to treat or prevent hypoxia resulting from blood loss (e.g., from acute hemorrhage or during surgical operations), resulting from anemia (e.g., pernicious anemia or sickle cell anemia), or resulting from shock (e.g., volume deficiency shock, anaphylactic shock, septic shock or allergic shock). The use of blood and blood fractions as in these capacities as a blood substitute is fraught with risks. For example, the use of whole blood often is accompanied by the risk of transmission of hepatitis-producing viruses and AIDS-producing viruses which can complicate patient recovery or result in patient fatalities. Additionally, the use of whole blood requires blood-typing and cross-matching to avoid immunohematological problems and interdonor incompatibility.

Human hemoglobin, as a blood substitute, possesses osmotic activity and the ability to transport and transfer oxygen, but it has the disadvantage of rapid elimination from circulation by the renal route and through vascular walls, resulting in a very short, and therefore, a typically unsatisfactory half-life. Further, human

hemoglobin is also frequently contaminated with toxic levels of endotoxins, bacteria and/or viruses.

Non-human hemoglobin suffers from the same deficiencies as human hemoglobin. In addition, hemoglobin from non-human sources is also typically contaminated with proteins, such as antibodies, which could cause an immune system response in the recipient.

Previously, at least four other types of blood substitutes have been utilized, including perfluorochemicals, synthesized hemoglobin analogues, liposome-encapsulated hemoglobin, and chemically-modified hemoglobin. However, many of these blood substitutes have typically had short intravascular retention times, being removed by the circulatory system as foreign substances or lodging in the liver, spleen, and other tissues. Also, many of these blood substitutes have been biologically incompatible with living systems.

Thus, in spite of the recent advances in the preparation of hemoglobin-based blood substitutes, the need has continued to exist for a blood substitute which has levels of contaminants, such as endotoxins, bacteria, viruses, phospholipids and non-hemoglobin proteins, which are sufficiently low to generally prevent an immune system response and any toxicological effects resulting from an infusion of the blood substitute. In addition, the blood substitute must also be capable of transporting and transferring adequate amounts of oxygen to tissues under ambient conditions and must have a good intravascular retention time.

Further, it is preferred that the blood substitute 1) has an oncotic activity generally equivalent to that of whole blood, 2) can be transfused to most recipients without cross-matching or sensitivity testing, and 3) can be stored with minimum amounts of refrigeration for long periods.

#### SUMMARY OF THE INVENTION

The present invention relates to a method for preserving a deoxygenated hemoglobin blood substitute and to a preserved deoxygenated blood substitute.

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The present invention is drawn to a method for preserving a deoxygenated hemoglobin blood substitute comprising maintaining the deoxygenated hemoglobin blood substitute in an oxygen barrier film primary package comprising a transparent laminate material, said film having an oxygen permeability of less than about 1.0 cc per 100 square inches (or about 0.155 cc per 100 square centimeters) per 24 hours per atmosphere at about 25°C and an external relative humidity of about 50%.

The present invention is also drawn to a preserved deoxygenated hemoglobin blood substitute. Said preserved blood substitute comprises a deoxygenated hemoglobin blood substitute and an oxygen barrier film primary package. Said oxygen barrier film primary package comprises a transparent laminate material, having an oxygen permeability of less than about 1.0 cc per 100 square inches (or about 0.155 cc per 100 square centimeters) per 24 hours per atmosphere at about 25°C and an external relative humidity of about 50%, within which the deoxygenated hemoglobin blood substitute is sealed, thereby preserving the deoxygenated hemoglobin blood substitute in an environment that is substantially free of oxygen.

One advantage of the present invention is that the hemoglobin produced and stored according to the methods of this invention has a greater degree of purity and longer shelf-life. A primary package having a high oxygen barrier allows the primary package to protect product stability before a high barrier overwrap is applied or after the overwrap is removed. In addition, transparent primary packaging allows the visual inspection of the production condition. Furthermore, present invention results in reduced plastic and medical waste by eliminating the need for additional barriers in the preservation of a hemoglobin blood substitute, additional barriers such as an overwrap.

The blood substitute can remain stable at room temperature for periods up to two years or more, a significant improvement over previous methods. Furthermore, with the purified hemoglobin of the present invention one species of hemoglobin can be successfully used as a blood substitute in a different species without the recipient species suffering significant side effects.

## DETAILED DESCRIPTION OF THE INVENTION

The features and other details of the process of the invention will now be more particularly described and pointed out in the claims. It will be understood that the particular embodiments of the invention are shown by way of example and not as limitations of the invention. The principle features of this invention can be employed in various embodiments without departing from the scope of the present invention.

In one embodiment, the invention relates to a method for preserving the stability of a deoxygenated hemoglobin blood substitute. This method includes maintaining deoxygenated hemoglobin blood substitute in an oxygen barrier film primary package. In one embodiment, the oxygen barrier film primary package includes a transparent polymer film having an oxygen permeability of less than about 1.0 cc per 100 square inches (or about 0.155 cc per 100 centimeters squared) per 24 hours per atmosphere at about 25° C and an external relative humidity of about 50%. Preferably, the primary package has a permeability of less than about 0.6 cc per 100 square inches (or about 0.093 cc per 100 centimeters squared) per 24 hours per atmosphere at 25° C. In another embodiment, the polymer film is a laminate.

In another embodiment, the invention relates to a preserved deoxygenated hemoglobin blood substitute that includes a deoxygenated blood substitute and an oxygen barrier film primary package. In one embodiment, the oxygen barrier film primary package includes a transparent polymer film. The primary package has an oxygen permeability of less than about 1.0 cc per 100 square inches (or about 0.155 cc per 100 square centimeters) per 24 hours per atmosphere at about 25°C and an external relative humidity of about 50%, within which the deoxygenated hemoglobin blood substitute is sealed, thereby preserving the deoxygenated hemoglobin blood substitute in an environment that is substantially free of oxygen. In another embodiment, the polymer film is a laminate.

The oxygen barrier film comprises suitable oxygen barrier material such that the material has suitable oxygen barrier properties at 25°C and ambient humidity,



5 for example 50% relative humidity. In one embodiment of the present invention, the  
oxygen barrier material comprises a transparent polymer film having at least one  
10 layer. In a more particular embodiment, the film comprises a laminate of an outer  
polyolefin layer (such as polyethylene or polypropylene), an oxygen barrier layer  
5 and an inner polyolefin layer, wherein the inner layer is in contact with the contents  
of the package. The polyolefins of the present invention can comprise copolymers  
15 of two or more monomers, wherein the monomers can be, for example,  
polypropylene, polyethethylene, or butylene. In another embodiment, other  
monomers such as ethylene vinyl acetate can be included in the copolymer.  
20 Depending upon the type of oxygen barrier layer, the laminate can optionally  
include a support layer. While not wishing to be bound by theory, the support layer  
facilitates the production of bags using an automated device. In a preferred  
25 embodiment, the support layer is a biaxially oriented material such as nylon. In one  
embodiment, the transparent material can be made to prevent photodegradation,  
15 using methods known in the art.

30 In one embodiment, the outer polyolefin layer and the oxygen barrier layer  
are co-extruded. In a preferred embodiment, the outer polyolefin layer is medium  
density polyethylene and the oxygen barrier layer is ethylene vinyl alcohol.

35 In another embodiment of the present invention, the oxygen barrier film  
20 comprises a co-extruded medium density polyethylene/ethylene vinyl alcohol layer  
having a thickness of about 0.0022 in. (or about 56 micrometers ( $\mu\text{m}$ )); a nylon layer  
having a thickness of about 0.00048 in. (or about 12.2  $\mu\text{m}$ ); and a low density  
40 polyethylene layer having a thickness of about 0.0020 in. (or about 50.8  $\mu\text{m}$ ).

While not wishing to be bound by theory, the inner and outer polyolefin  
25 layers are vapor barriers. The vapor barrier properties of either layer can be  
increased by increasing the thickness of the layer. It is not necessary to have a vapor  
45 barrier on the outside of the package, however, for the purpose of automated  
production of sterile bags, it is desirable to have an outer polyolefin layer, such as a  
medium density polyethylene layer, because this layer protects the stability of the  
50 oxygen barrier layer during the sterilization process. For example, this layer  
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protects the oxygen barrier layer during the process of pulling the film through a hydrogen peroxide bath. Other suitable outer layers include, for example, linear low density polyethylene, low density polyethylene, high density polyethylene, or polypropylenes. It is understood, for example, that if no sterilization procedures are required, the outer polyolefin layer would not be required. In addition, if different sterilization techniques are used wherein the oxygen barrier layer is not affected, or where an oxygen barrier layer that withstands the sterilization process is used, an outer polyolefin layer is not required.

In another embodiment of the present invention, the oxygen barrier layer comprises an essentially oxygen-impermeable polymer, comprising a coated support material. In one embodiment, the support material can be, for example, polyester or polyamide (such as nylon) and the coating can be, for example, silicon oxide ( $\text{SiO}_2$ ) or other material, such as a metal oxide, that can be deposited onto the support to render it oxygen impermeable.

Optionally, an overwrap can be employed. The overwrap is manufactured from a suitable material, such as polymer films, (e.g., an essentially oxygen-impermeable polyester, polypropylene, ethylene vinyl alcohol (EVOH), or nylon) or a laminate, such as a foil laminate (e.g., a silver or aluminum foil laminate) or other oxygen barrier laminate. Where the overwrap is a film, such as a polyester film, the film can be rendered essentially oxygen-impermeable by a variety of suitable methods. In one embodiment, the film as manufactured is essentially oxygen-impermeable. Alternatively, where the polymeric material is not sufficiently oxygen-impermeable to meet the desired specifications, the film can be laminated or otherwise treated to reduce or eliminate the oxygen permeability. In a preferred embodiment, a foil laminate is employed where the foil is an aluminum, silver, gold or other metal. The foil layer preferably has a thickness between about 0.0001 and 0.001 inches (or about 2.54 and 25.4  $\mu\text{m}$ ), more preferably about 0.0003 inches (or about 7.62  $\mu\text{m}$ ). The laminate typically contains one or more polymeric layers. The polymer can be a variety of polymeric materials including, for example, a polyester

layer (e.g., a 48 gauge polyester, or about 12.2  $\mu\text{m}$ ), nylon, ethylene vinyl alcohol, polyvinylidene chloride, etc.

The primary package and the overwrap, if present, can be of a variety of constructions, including vials, cylinders, boxes, etc. In a preferred embodiment, the primary package is in the form of a bag. A suitable bag can be formed by, for example, continuously bonding one or more (e.g., two) sheets at the perimeter(s) thereof to form a tightly closed, oxygen impermeable, construction having a fillable center. The bonding can be achieved with any suitable material. Where linear low, low, medium or high density polyethylene is used as the inner layer of the material, the sheets can be sealed by heating under the appropriate conditions. It is well known in the art that polyethylene can be sealed against itself with heat under the appropriate conditions. It is well known in the art that parameters can be varied to obtain proper bonding of polyolefin surfaces of film, these parameters include temperature, pressure and "dwell time", wherein dwell time is the duration of time the sheets are put under pressure and temperature. Typically, linear low density polyethylene requires less heat and progressively higher density polypropylene requires progressively more heat. For example, a laminate material having 1.5 mil (0.0015 in. or 38.1  $\mu\text{m}$ ) linear low density polyethylene on the inner surface of two sheets exposed to 300°F (149°C), at 50 psi (34.47 Newton/cm<sup>2</sup>), for 1 second results in a seal suitable in the method of the present invention. In addition, higher density polyolefins typically tolerate higher pressure during the bonding process. In general, if the pressure is excessive, the heated material may be forced away from the area of contact, creating a weaker seal. In the case of a polyester/foil laminate material, a polyester adhesive can be employed for example.

In a preferred embodiment, the blood substitute is packaged under an atmosphere which is substantially free of oxygen. Examples of suitable atmospheres include nitrogen, argon and helium.

As defined herein, a blood substitute is a hemoglobin-based oxygen carrying composition for use in humans, mammals and other vertebrates, which is capable of transporting and transferring oxygen to vital organs and tissues, at least, and can

maintain sufficient intravascular oncotic pressure. A vertebrate is as classically defined, including humans, or any other vertebrate animals which uses blood in a circulatory system to transfer oxygen to tissue. Additionally, the definition of circulatory system is as classically defined, consisting of the heart, arteries, veins and microcirculation including smaller vascular structures such as capillaries.

A blood substitute of the invention preferably has levels of endotoxins, phospholipids, foreign proteins and other contaminants which will not result in a significant immune system response and which are non-toxic to the recipient. Preferably, a blood substitute is ultrapure. Ultrapure as defined herein, means containing less than 0.5 EU/ml of endotoxin, less than 3.3 nmoles/ml phospholipids and little to no detectable levels of non-hemoglobin proteins, such as serum albumin or antibodies.

The term "endotoxin" refers to the cell-bound lipopolysaccharides, produced as a part of the outer layer of gram-negative bacterial cell walls, which under many conditions are toxic. When injected into animals, endotoxins can cause fever, diarrhea, hemorrhagic shock, and other tissue damage. Endotoxin unit (EU) has been defined by the United States Pharmacopeial Convention of 1983, page 3014, as the activity contained in 0.1 nanograms of U.S. reference standard lot EC-5. One vial of EC-5 contains 10,000 EU. Examples of suitable means for determining endotoxin concentrations in a blood substitute include the method "Kinetic/Turbidimetric Limulus Amebocytic Lystate (LAL) 5000 Methodology" developed by Associates of Cape Cod, Woods Hole, Massachusetts.

Stable polymerized hemoglobin, as defined herein, is a hemoglobin-based oxygen carrying composition which does not substantially increase or decrease in molecular weight distribution and/or in methemoglobin content during storage periods at suitable storage temperatures for periods of two years or more, and preferably for periods of two years or more, when stored in a low oxygen environment. Suitable storage temperatures for storage of one year or more are between about 0°C and about 40°C. The preferred storage temperature range is between about 0°C and about 25°C.

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A suitable low oxygen environment, or an environment that is substantially oxygen-free, is defined as the cumulative amount of oxygen in contact with the blood substitute, over a storage period of at least about two months, preferably at least about one year, or more preferably at least about two years which will result in a methemoglobin concentration of less than about 15% by weight in the blood substitute. The cumulative amount of oxygen includes oxygen inleakage into the blood substitute packaging and the original oxygen content of the blood substitute and packaging.

Throughout this method, from red blood cell (RBC) collection until hemoglobin polymerization, blood solution, RBCs and hemoglobin are maintained under conditions sufficient to minimize microbial growth, or bioburden, such as maintaining temperature at less than about 20°C and above 0°C. Preferably, temperature is maintained at a temperature of about 15°C or less. More preferably, the temperature is maintained at 10 ± 2°C.

In this method, portions of the components for the process for preparing a stable polymerized hemoglobin blood substitute are sufficiently sanitized to produce a sterile product. Sterile is as defined in the art, specifically, that the solution meets United States Pharmacopeia requirements for sterility provided in *USP XXII*, Section 71, pages 1483-1488. Further, portions of components that are exposed to the process stream, are usually fabricated or clad with a material that will not react with or contaminate the process stream. Such materials can include stainless steel and other steel alloys, such as Inconel.

Suitable RBC sources include human blood, bovine blood, ovine blood, porcine blood, blood from other vertebrates and transgenically-produced hemoglobin, such as the transgenic Hb described in *BIO/TECHNOLOGY*, 12: 55-59 (1994).

The blood can be collected from live or freshly slaughtered donors. One method for collecting bovine whole blood is described in U.S. Patent Nos. 5,084,558

and 5,296,465, issued to Rausch *et al.* It is preferred that the blood be collected in a sanitary manner.

At or soon after collection, the blood is mixed with at least one anticoagulant to prevent significant clotting of the blood. Suitable anticoagulants for blood are as classically known in the art and include, for example, sodium citrate, ethylenediaminetetraacetic acid and heparin. When mixed with blood, the anticoagulant may be in a solid form, such as a powder, or in an aqueous solution.

It is understood that the blood solution source can be from a freshly collected sample or from an old sample, such as expired human blood from a blood bank.

Further, the blood solution could previously have been maintained in frozen and/or liquid state. It is preferred that the blood solution is not frozen prior to use in this method.

In another embodiment, prior to introducing the blood solution to anticoagulants, antibiotic levels in the blood solution, such as penicillin, are assayed. Antibiotic levels are determined to provide a degree of assurance that the blood sample is not burdened with an infecting organism by verifying that the donor of the blood sample was not being treated with an antibiotic. Examples of suitable assays for antibiotics include a penicillin assay kit (Difco, Detroit, MI) employing a method entitled "Rapid Detection of Penicillin in Milk". It is preferred that blood solutions contain a penicillin level of less than or equal to about 0.008 units/ml. Alternatively, a herd management program to monitor the lack of disease in or antibiotic treatment of the cattle may be used.

Preferably, the blood solution is strained prior to or during the anticoagulation step, for example by straining, to remove large aggregates and particles. A 600 mesh screen is an example of a suitable strainer.

The RBCs in the blood solution are then washed by suitable means, such as by diafiltration or by a combination of discrete dilution and concentration steps with at least one solution, such as an isotonic solution, to separate RBCs from extracellular plasma proteins, such as serum albumins or antibodies (e.g.,

immunoglobulins (IgG)). It is understood that the RBCs can be washed in a batch or continuous feed mode.

Acceptable isotonic solutions are as known in the art and include solutions, such as a citrate/saline solution, having a pH and osmolarity which does not rupture the cell membranes of RBCs and which displaces the plasma portion of the whole blood. A preferred isotonic solution has a neutral pH and an osmolarity between about 285-315 mOsm. In a preferred embodiment, the isotonic solution is composed of an aqueous solution of sodium citrate dihydrate (6.0 g/l) and of sodium chloride (8.0 g/l).

Water which can be used in the method of invention includes distilled water, deionized water, water-for-injection (WFI) and/or low pyrogen water (LPW). WFI, which is preferred, is deionized, distilled water that meets U.S. Pharmacological Specifications for water-for-injection. WFI is further described in *Pharmaceutical Engineering*, 11, 15-23 (1991). LPW, which is preferred, is deionized water containing less than 0.002 EU/ml.

It is preferred that the isotonic solution be filtered prior to being added to the blood solution. Examples of suitable filters include a Millipore 10,000 Dalton ultrafiltration membrane, such as a Millipore Cat # CDUF 050 G1 filter or A/G Technology hollow fiber, 10,000 Dalton (Cat # UFP-10-C-85).

In a preferred embodiment, RBCs in the blood solution are washed by diafiltration. Suitable diafilters include microporous membranes with pore sizes which will separate RBCs from substantially smaller blood solution components, such as a 0.1  $\mu\text{m}$  to 0.5  $\mu\text{m}$  filter (e.g., a 0.2  $\mu\text{m}$  hollow fiber filter, Microgon Krosflo II microfiltration cartridge). Concurrently, a filtered isotonic solution is added continuously (or in batches) as makeup at a rate equal to the rate (or volume) of filtrate lost across the diafilter. During RBC washing, components of the blood solution which are significantly smaller in diameter than RBCs, or are fluids such as plasma, pass through the walls of the diafilter in the filtrate. RBCs, platelets and larger bodies of the diluted blood solution, such as white blood cells, are retained

and mixed with isotonic solution, which is added continuously or batchwise to form a dialyzed blood solution.

In a more preferred embodiment, the volume of blood solution in the diafiltration tank is initially diluted by the addition of a volume of a filtered isotonic solution to the diafiltration tank. Preferably, the volume of isotonic solution added is about equal to the initial volume of the blood solution.

In an alternate embodiment, the RBCs are washed through a series of sequential (or reverse sequential) dilution and concentration steps, wherein the blood solution is diluted by adding at least one isotonic solution, and is concentrated by flowing across a filter, thereby forming a dialyzed blood solution.

RBC washing is complete when the level of plasma proteins contaminating the RBCs has been substantially reduced (typically at least about 90%). Typically, RBC washing is complete when the volume of filtrate drained from diafilter 34 equals about 300%, or more, of the volume of blood solution contained in the diafiltration tank prior to diluting the blood solution with filtered isotonic solution. Additional RBC washing may further separate extracellular plasma proteins from the RBCs. For instance, diafiltration with 6 volumes of isotonic solution may remove at least about 99% of IgG from the blood solution.

The dialyzed blood solution is then exposed to means for separating the RBCs in the dialyzed blood solution from the white blood cells and platelets, such as by centrifugation.

It is understood that other methods generally known in the art for separating RBCs from other blood components can be employed. For example, sedimentation, wherein the separation method does not rupture the cell membranes of a significant amount of the RBCs, such as less than about 30% of the RBCs, prior to RBC separation from the other blood components.

Following separation of the RBCs, the RBCs are lysed by a means for lysing RBCs to release hemoglobin from the RBCs to form a hemoglobin-containing solution. Lysis means can use various lysis methods, such as mechanical lysis, chemical lysis, hypotonic lysis or other known lysis methods which release



hemoglobin without significantly damaging the ability of the Hb to transport and release oxygen.

In yet another embodiment, recombinantly produced hemoglobin, such as the recombinantly produced hemoglobin described in *Nature*, 356: 258-260 (1992), can be processed in the method of invention in place of RBCs. The bacteria cells containing the hemoglobin are washed and separated from contaminants as described above. These bacteria cells are then mechanically ruptured by means known in the art, such as a ball mill, to release hemoglobin from the cells and to form a lysed cell phase. This lysed cell phase is then processed as is the lysed RBC phase.

Following lysis, the lysed RBC phase is then ultrafiltered to remove larger cell debris, such as proteins with a molecular weight above about 100,000 Daltons. Generally, cell debris include all whole and fragmented cellular components with the exception of Hb, smaller cell proteins, electrolytes, coenzymes and organic metabolic intermediates. Acceptable ultrafilters include, for example, 100,000 Dalton filters made by Millipore (Cat.# CDUF 050 H1) and made by A/G Technology (Needham, MA.; Model No. UFP100E55).

It is preferred that ultrafiltration continues until the concentration of Hb in the lysed RBC phase is less than 8 grams/liter (g/l) to maximize the yield of hemoglobin available for polymerization. Other methods for separating Hb from the lysed RBC phase can be employed, including sedimentation, centrifugation or microfiltration.

The Hb ultrafiltrate can then be ultrafiltered to remove smaller cell debris, such as electrolytes, coenzymes, metabolic intermediates and proteins less than about 30,000 Daltons in molecular weight, and water from the Hb ultrafiltrate. Suitable ultrafilters include a 30,000 Dalton ultrafilter (Millipore Cat # CDUF 050 T1 and/or Armicon, # 540 430).

The concentrated Hb solution can then be directed into one or more parallel chromatographic columns to further separate the hemoglobin by high performance liquid chromatography from other contaminants such as antibodies, endotoxins,

phospholipids and enzymes and viruses. Examples of suitable media include anion exchange media, cation exchange media, hydrophobic interaction media and affinity media. In a preferred embodiment, chromatographic columns contain an anion exchange medium suitable to separate Hb from non-hemoglobin proteins. Suitable anion exchange mediums include, for example, silica, alumina, titania gel, cross-linked dextran, agarose or a derivatized moiety, such as a polyacrylamide, a polyhydroxyethyl-methacrylate or a styrene divinylbenzene, that has been derivatized with a cationic chemical functionality, such as a diethylaminoethyl or quaternary aminoethyl group. A suitable anion exchange medium and corresponding eluants for the selective absorption and desorption of Hb as compared to other proteins and contaminants, which are likely to be in a lysed RBC phase, are readily determinable by one of reasonable skill in the art.

In a more preferred embodiment, a method is used to form an anion exchange media from silica gel, which is hydrothermally treated to increase the pore size, exposed to  $\gamma$ -glycidoxy propylsilane to form active epoxide groups and then exposed to  $C_3H_7(CH_3)NCl$  to form a quaternary ammonium anion exchange medium. This method is described in the *Journal of Chromatography*, 120:321-333 (1976).

Chromatographic columns are first pre-treated by flushing with a first eluant which facilitates Hb binding. Concentrated Hb solution is then injected onto the medium in the columns. After injecting the concentrated Hb solution, the chromatographic columns are then successively washed with different eluants to produce a separate, purified Hb eluate.

In a preferred embodiment, a pH gradient is used in chromatographic columns to separate protein contaminants, such as the enzyme carbonic anhydrase, phospholipids, antibodies and endotoxins from the Hb. Each of a series of buffers having different pH values, are sequentially directed to create a pH gradient within the medium in the chromatographic column. It is preferred that the buffers be filtered, such as with a 10,000 Dalton depyrogenation membrane. The buffers used to separate Hb should have a low ionic strength such that elution of Hb and non-

hemoglobin contaminants is generally dependent upon pH and not significantly dependent upon ionic strength. Typically, buffers with an ionic concentration of about 50 mM, or less, have suitable low ionic strengths.

The first buffer transports the concentrated Hb solution into the medium in the chromatographic columns and facilitates binding of the Hb to the medium. The second buffer then adjusts the pH within the columns to elute contaminating non-hemoglobin components while maintaining the Hb bound to the medium. The third buffer then elutes the Hb. The Hb eluate is then collected. It is preferred that the Hb eluate be directed through a sterile filter. Suitable sterile filters include 0.22  $\mu$ m filters, such as a Sartorius Sartobran Cat # 5232507 G1PH filter.

In a preferred embodiment, the first 3%-to-4% of the Hb eluate and the last 3%-to-4% of the Hb eluate are directed to waste to provide assurance of the purity of the Hb eluate.

Wherein the chromatographic columns are to be reused, contaminating non-hemoglobin proteins and endotoxin, remaining in the columns, are then eluted by a fourth buffer.

The use of pH gradients to separate Hb from non-hemoglobin contaminants is further described in U.S. Patent 5,691,452, filed June 7, 1995. In a preferred embodiment, the first buffer is a tris-hydroxymethyl aminomethane (Tris) solution (concentration about 20mM; pH about 8.4 to about 9.4). The second buffer is a mixture of the first buffer and a third buffer, with the second buffer having a pH of about 8.2 to about 8.6. The third buffer is a Tris solution (concentration about 50 mM; pH about 6.5 to about 7.5). The fourth buffer is a NaCl/Tris solution (concentrations about 1.0 M NaCl and about 20 mM Tris; pH about 8.4 to about 9.4, preferably about 8.9-9.1). It is particularly preferred that the pH of the second buffer be between about 8.2 and about 8.4.

Typically, the buffers used are at a temperature between about 0°C and about 50°C. Preferably, buffer temperature is about  $12.4 \pm 1.0^\circ\text{C}$  during use. In addition, the buffers are typically stored at a temperature of about 9°C to about 11°C.

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The Hb eluate is then preferably deoxygenated prior to polymerization to form a deoxygenated Hb solution (hereinafter deoxy-Hb) by means that substantially deoxygenate the Hb without significantly reducing the ability of the Hb in the Hb eluate to transport and release oxygen, such as would occur from denaturation of formation of oxidized hemoglobin (methHb).

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In one embodiment, the Hb eluate is deoxygenated by gas transfer of an inert gas across a phase membrane. Such inert gases include, for example, nitrogen, argon and helium. It is understood that other means for deoxygenating a solution of hemoglobin, which are known in the art, can be used to deoxygenate the Hb eluate. Such other means, can include, for example, nitrogen sparging of the Hb eluate, chemical scavenging with reducing agents such as N-acetyl-L-cysteine (NAC), cysteine, sodium dithionite or ascorbate, or photolysis by light.

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Following elution from the chromatographic column, the Hb eluate is preferably concentrated to improve the efficiency of the process. The Hb eluate is recirculated through an ultrafilter to concentrate the Hb eluate to form a concentrated Hb solution. Suitable ultrafilters include, for example, 30,000 or less Dalton ultrafilters (e.g., Millipore Helicon, Cat # CDUF050G1 or Amicon Cat # 540430). Typically, concentration of the Hb eluate is complete when the concentration of Hb is between about 100 to about 120 g/l. While concentrating the Hb eluate, the Hb eluate temperature is preferably maintained at approximately 8-12°C.

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Buffer is then directed into the Hb solution, which is preferably concentrated, to adjust the ionic strength of the Hb solution to enhance Hb deoxygenation. It is preferred that the ionic strength be adjusted to between about 150 meq/l and about 200 meq/l to reduce the oxygen affinity of the Hb in the Hb solution. Suitable buffers include buffers with a pH that will not result in significant denaturing of the Hb protein but will have an ionic strength sufficiently high to promote Hb deoxygenation. Examples of suitable buffers include saline solutions with a pH range of about 6.5 to about 8.9. A preferred buffer is an aqueous 1.0 M NaCl, 20 mM Tris solution with a pH of about 8.9.

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Preferably, the resulting buffered Hb solution is then recirculated through the ultrafilter, to again concentrate the Hb solution to improve the efficiency of the process. In a preferred embodiment, concentration is complete when the concentration of Hb is about 100 g/l to about 120 g/l.

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5 During deoxygenation the Hb solution is circulated through a suitable phase transfer membrane. Appropriate phase transfer membranes include, for example, a 0.05  $\mu\text{m}$  polypropylene hollow fiber microfilter (e.g., Hoechst-Celanese Cat # 5PCM-107). Concurrently, a counterflow of an inert gas is passed across the phase transfer membrane. Suitable inert gases include, for example, nitrogen, argon and 10 helium. Gas exchange across the phase transfer membrane thereby strips oxygen out of the Hb solution.

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Deoxygenation continues until the  $\text{pO}_2$  of the Hb solution is reduced to a level wherein the oxygenated Hb (oxyhemoglobin or  $\text{HbO}_2$ ) content in the Hb solution is about 20% or less. In a preferred embodiment, the  $\text{HbO}_2$  content in the 15 Hb solution is about 10% or less.

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During deoxygenation, the temperature of the Hb solution is typically maintained at a level that will balance the rate of deoxygenation against the rate of methemoglobin formation. Temperature is maintained to limit methemoglobin content to less than 20%. An optimum temperature will result in less than about 5% 20 methemoglobin content, and preferably less than about 2.5% methemoglobin content, while still deoxygenating the Hb solution. Typically, during deoxygenation the temperature of the Hb solution is maintained between about 19 °C and about 31°C.

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During deoxygenation, and subsequently throughout the remaining steps of 25 the method of invention, the Hb is maintained in a low oxygen environment to minimize oxygen absorption by the Hb and to maintain an  $\text{HbO}_2$  content of less than about 20%, preferably less than about 10%.

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The deoxygenated-Hb is then preferably equilibrated with a low oxygen content storage buffer, containing a sulfhydryl compound, to form an oxidation-stabilized deoxy-Hb. Suitable sulfhydryl compounds include non-toxic reducing 30

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agents, such as N-acetyl-L-cysteine (NAC) D,L-cysteine,  $\gamma$ -glutamyl-cysteine, glutathione, 2,3-dimercapto-1-propanol, 1,4-butanedithiol, thioglycolate, and other biologically compatible sulfhydryl compounds. The oxygen content of a low oxygen content storage buffer must be low enough not to significantly reduce the concentration of sulfhydryl compound in the buffer and to limit oxyhemoglobin content in oxidation stabilized deoxy-Hb to about 20% or less, preferably less than about 10%. Typically, the storage buffer has a  $pO_2$  of less than about 50 torr.

In a preferred embodiment, the storage buffer should have a pH suitable to balance Hb polymerization and methemoglobin formation, typically between about 7.6 and about 7.9.

The amount of a sulfhydryl compound mixed with the deoxy-Hb is an amount high enough to increase intramolecular cross-linking of Hb during polymerization and low enough not to significantly decrease intermolecular cross-linking of Hb molecules, due to a high ionic strength. Typically, about one mole of sulfhydryl functional groups (-SH) are needed to oxidation stabilize between about 0.25 moles to about 5 moles of deoxy-Hb.

In a preferred embodiment, the storage buffer contains approximately 25-35 mM sodium phosphate buffer (pH 7.7-7.8) and contains an amount of NAC such that the concentration of NAC in oxidation stabilized deoxy-Hb is between about 0.003% and about 0.3%, by weight. More preferably, the NAC concentration in the oxidation stabilized deoxy-Hb is between about 0.05% and about 0.2% by weight.

Preferably, the storage buffer is filtered prior to mixing with the deoxy-Hb, such as through a 10,000 Dalton ultrafiltration membrane (Millipore Helicon Cat # CDUF050G1 or A/G Technology Maxcell Cat # UFP-10-C-75).

In one embodiment, the oxidation-stabilized deoxy-Hb then flows through an optional filter. Suitable filters include a 0.2  $\mu$ m polypropylene prefilter and a 0.5  $\mu$ m sterile microfilter (Pall Profile II, Cat # ABIY005Z7 or Gelman Supor). The deoxy-Hb is maintained under a substantially oxygen-free atmosphere. This can be accomplished, for example, by purging and blanketing the process apparatus with an

inert gas, such as nitrogen, prior to and after filling with oxidation-stabilized deoxy-Hb.

Optionally, prior to transferring the oxidation-stabilized deoxy-Hb to polymerization, an appropriate amount of water is added to the polymerization reactor. In one embodiment an appropriate amount of water is that amount which would result in a solution with a concentration of about 10 to about 100 g/l Hb when the oxidation-stabilized deoxy-Hb is added to the polymerization reactor. Preferably, the water is oxygen-depleted.

After the  $pO_2$  of the water in the polymerization step is reduced to a level sufficient to limit  $HbO_2$  content to about 20%, typically less than about 50 torr, the polymerization reactor is blanketed with an inert gas, such as nitrogen. The oxidation-stabilized deoxy-Hb is then transferred into the polymerization reactor, which is concurrently blanketed with an appropriate flow of an inert gas.

The temperature of the oxidation-stabilized deoxy-Hb solution in polymerization reactor is raised to a temperature to optimize polymerization of the oxidation-stabilized deoxy-Hb when contacted with a cross-linking agent. Typically, the temperature of the oxidation-stabilized deoxy-Hb is about 25°C to about 45°C, and preferably about 41°C to about 43°C throughout polymerization. An example of an acceptable heat transfer means for heating the polymerization reactor is a jacketed heating system which is heated by directing hot ethylene glycol through the jacket.

The oxidation-stabilized deoxy-Hb is then exposed to a suitable cross-linking agent at a temperature sufficient to polymerize the oxidation-stabilized deoxy-Hb to form a solution of polymerized hemoglobin (poly(Hb)) over a period of about 2 hours to about 6 hours.

Examples of suitable cross-linking agents include polyfunctional agents that will cross-link Hb proteins, such as glutaraldehyde, succindialdehyde, activated forms of polyoxyethylene and dextran,  $\alpha$ -hydroxy aldehydes, such as glycolaldehyde, N-maleimido-6-aminocaproyl-(2'-nitro,4'-sulfonic acid)-phenyl ester, m-maleimidobenzoic acid-N-hydroxysuccinimide ester, succinimidyl 4-(N-

maleimidomethyl)cyclohexane-1-carboxylate, sulfosuccinimidyl 4-(N-maleimidomethyl)cyclohexane-1-carboxylate, m-maleimido benzoyl-N-hydroxysuccinimide ester, m-maleimido benzoyl-N-hydroxysulfosuccinimide ester, N-succinimidyl(4-iodoacetyl)aminobenzoate, sulfosuccinimidyl(4-iodoacetyl)aminobenzoate, succinimidyl 4-(p-maleimidophenyl)butyrate, sulfosuccinimidyl 4-(p-maleimidophenyl)butyrate, 1-ethyl-3-(3-dimethylaminopropyl)carbodiimide hydrochloride, N,N'-phenylene dimaleimide, and compounds belonging to the bis-imidate class, the acyl diazide class or the aryl dihalide class, among others.

A suitable amount of a cross-linking agent is that amount which will permit intramolecular cross-linking to stabilize the Hb and also intermolecular cross-linking to form polymers of Hb, to thereby increase intravascular retention. Typically, a suitable amount of a cross-linking agent is that amount wherein the molar ratio of cross-linking agent to Hb is in excess of about 2:1. Preferably, the molar ratio of cross-linking agent to Hb is between about 20:1 to 40:1.

Preferably, the polymerization is performed in a buffer with a pH between about 7.6 to about 7.9, having a chloride concentration less than or equal to about 35 mmolar.

In a preferred embodiment, a suitable amount of the cross-linking agent is added to the oxidation-stabilized deoxy-Hb and then mixed by a means for mixing with low shear. A suitable low-shear mixing means includes a static mixer. A suitable static mixer is, for example, a "Kenics" static mixer obtained from Chemineer, Inc.

In one embodiment, recirculating the oxidation-stabilized deoxy-Hb and the cross-linking agent through the static mixer causes turbulent flow conditions with generally uniform mixing of the cross-linking agent with the oxidation-stabilized deoxy-Hb thereby reducing the potential for forming pockets of deoxy-Hb containing high concentrations of the cross-linking agent. Generally uniform mixing of the cross-linking agent and the deoxy-Hb reduces the formation of high molecular weight Hb polymers, i.e. polymers weighing more than 500,000 Daltons,



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and also permits faster mixing of the cross-linking agent and the deoxy-Hb during polymerization. Furthermore, significant Hb intramolecular cross-linking will result during Hb polymerization due to the presence of a sulfhydryl compound, preferably NAC. While the exact mechanism of the interaction of the sulfhydryl compound with glutaraldehyde and/or Hb is not known, it is presumed that the sulfhydryl compound affects Hb/cross-linking agent chemical bonding in a manner that at least partially inhibits the formation of high molecular weight Hb polymers and preferentially forms stabilized tetrameric Hb.

Poly(Hb) is defined as having significant intramolecular cross-linking if a substantial portion (e.g., at least about 50%) of the Hb molecules are chemically bound in the poly(Hb), and only a small amount, such as less than about 15% are contained within high molecular weight polymerized hemoglobin chains. High molecular weight poly(Hb) molecules are molecules, for example, with a molecular weight above about 500,000 Daltons.

In a preferred embodiment, glutaraldehyde is used as the cross-linking agent. Typically, about 10 to about 70 grams of glutaraldehyde are used per kilogram of oxidation-stabilized deoxy-Hb. More preferably, glutaraldehyde is added over a period of five hours until approximately 29-31 grams of glutaraldehyde are added for each kilogram of oxidation-stabilized deoxy-Hb.

After polymerization, the temperature of the poly(Hb) solution in polymerization reactor is typically reduced to about 15°C to about 25°C.

Wherein the cross-linking agent used is not an aldehyde, the poly(Hb) formed is generally a stable poly(Hb). Wherein the cross-linking agent used is an aldehyde, the poly(Hb) formed is generally not stable until mixed with a suitable reducing agent to reduce less stable bonds in the poly(Hb) to form more stable bonds. Examples of suitable reducing agents include sodium borohydride, sodium cyanoborohydride, sodium dithionite, trimethylamine, t-butylamine, morpholine borane and pyridine borane. Prior to adding the reducing agent, the poly(Hb) solution is optionally concentrated by ultrafiltration until the concentration of the poly(Hb) solution is increased to between about 75 and about 85 g/l. An example of

a suitable ultrafilter is a 30,000 Dalton filter (e.g., Millipore Helicon, Cat # CDUF050LT and Amicon, Cat # 540430).

The pH of the poly(Hb) solution is then adjusted to the alkaline pH range to preserve the reducing agent and to prevent hydrogen gas formation, which can denature Hb during the subsequent reduction. In one embodiment, the pH is adjusted to greater than 10. The pH can be adjusted by adding a buffer solution to the poly(Hb) solution during or after polymerization. The poly(Hb) is typically purified to remove non-polymerized hemoglobin. This can be accomplished by diafiltration or hydroxyapatite chromatography (see, e.g. U.S. Patent 5,691,453).

Following pH adjustment, at least one reducing agent, preferably a sodium borohydride solution, is added to the polymerization step typically through the deoxygenation loop. Typically, about 5 to about 18 moles of reducing agent are added per mole of Hb tetramer (per 64,000 Daltons of Hb) within the poly(Hb). In a preferred embodiment, for every nine liters of poly(Hb) solution in polymerization subsystem 98, one liter of 0.25 M sodium borohydride solution is added at a rate of 0.1 to 0.12 lpm.

The pH and electrolytes of the stable poly(Hb) can then be restored to physiologic levels to form a stable polymerized hemoglobin blood substitute, by diafiltering the stable poly(Hb) with a diafiltration solution having a suitable pH and physiologic electrolyte levels. Preferably, the diafiltration solution is a buffer solution.

Wherein the poly(Hb) was reduced by a reducing agent, the diafiltration solution has an acidic pH, preferably between about 4 to about 6.

A non-toxic sulfhydryl compound can also be added to the stable poly(Hb) solution as an oxygen scavenger to enhance the stability of the final polymerized hemoglobin blood substitute. The sulfhydryl compound can be added as part of the diafiltration solution and/or can be added separately. An amount of sulfhydryl compound is added to establish a sulfhydryl concentration which will scavenge oxygen to maintain methemoglobin content less than about 15% over the storage period. Preferably, the sulfhydryl compound is NAC. Typically, the amount of

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sulphydryl compound added is an amount sufficient to establish a sulphydryl concentration between about 0.05% and about 0.2% by weight.

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In a preferred embodiment, the blood substitute is packaged under aseptic handling conditions while maintaining pressure with an inert, substantially oxygen-free atmosphere, in the polymerization reactor and remaining transport apparatus.

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The specifications for a suitable stable polymerized hemoglobin blood substitute formed by the method of invention are provided in Table I.

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Table I

PARAMETER	RESULTS
pH (18-22°C)	Physiologically acceptable
Endotoxin	Physiologically acceptable
Sterility Test	Meets Test
Phospholipids <sup>a</sup>	Physiologically acceptable
Total Hemoglobin	10 - 250 g/l
Methemoglobin	<15%
Oxyhemoglobin	<10%
Sodium, Na <sup>+</sup>	Physiologically acceptable
Potassium, K <sup>+</sup>	
Chloride, Cl <sup>-</sup>	
Calcium, Ca <sup>++</sup>	
Boron	
Glutaraldehyde	Physiologically acceptable
N-acetyl-L-cysteine	Physiologically Acceptable
M.W. >500,000	≤ 15%
M.W. ≤ 65,000	<10%
M.W. <32,000	<5%
Particulate Content >10μ	<12/ml
Particulate Content >25μ	<2/ml

a - measured in Hb before polymerization

The stable blood substitute is then stored in a short-term storage container or into sterile storage containers, each having a low oxygen environment as described in detail above. The storage container should also be sufficiently impermeable to water vapor passage to prevent significant concentration of the blood substitute by

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10 evaporation over the storage period. Significant concentration of the blood substitute is concentration resulting in one or more parameters of the blood substitute being high out of specification.

15 The synthesis of a stable polymerized hemoglobin blood substitute, formed according to the method of invention, is further described in U.S. Patent No. 5,296,465.

20 Vertebrates which can receive the blood substitute, formed by the methods of the invention include mammals, such as a human, non-human primate, a dog, a cat, a rat, a horse or a sheep. Further, vertebrates, which can receive said blood substitute, includes fetuses (prenatal vertebrate), post-natal vertebrates, or vertebrates at time of birth.

25 A blood substitute of the present invention can be administered into the circulatory system by injecting the blood substitute directly and/or indirectly into the circulatory system of the vertebrate, by one or more injection methods. Examples of direct injection methods include intravascular injections, such as intravenous and intra-arterial injections, and intracardiac injections. Examples of indirect injection methods include intraperitoneal injections, subcutaneous injections, such that the blood substitute will be transported by the lymph system into the circulatory system or injections into the bone marrow by means of a trocar or catheter. Preferably, the blood substitute is administered intravenously.

35 The vertebrate being treated can be normovolemic, hypervolemic or hypovolemic prior to, during, and/or after infusion of the blood substitute. The blood substitute can be directed into the circulatory system by methods such as top loading and by exchange methods.

40 25 A blood substitute can be administered therapeutically, to treat hypoxic tissue within a vertebrate resulting from many different causes including reduced RBC flow in a portion of, or throughout, the circulatory system, anemia and shock. Further, the blood substitute can be administered prophylactically to prevent oxygen-depletion of tissue within a vertebrate, which could result from a possible or expected reduction in RBC flow to a tissue or throughout the circulatory system of the vertebrate. Further discussion of the administration of hemoglobin to therapeutically or prophylactically treat hypoxia, particularly from a partial arterial obstruction or from a partial blockage in microcirculation, and the dosages used

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therein, is provided in copending U.S. Patent Application Serial No. 08/409,337, filed March 23, 1995, now U.S. Patent 5,854,209.

Typically, a suitable dose, or combination of doses of blood substitute, is an amount which when contained within the blood plasma will result in a total hemoglobin concentration in the vertebrate's blood between about 0.1 to about 10 grams Hb/dl, or more, if required to make up for large volume blood losses.

The invention will now be further and specifically described by the following examples.

#### Example 1

##### Synthesis of Stable Polymerized Hb Blood substitute

As described in U.S. Patent No. 5,296,465, samples of bovine whole blood were collected, mixed with a sodium citrate anticoagulant to form a blood solution.

Each blood solution sample was maintained after collection at a temperature of about 2°C and then strained to remove large aggregates and particles with a 600 mesh screen.

Prior to pooling, the penicillin level in each blood solution sample was assayed with an assay kit purchased from Difco, Detroit, Michigan using the method entitled "Rapid Detection of Penicillin in Milk" to ensure that penicillin levels in the blood solutions were < 0.008 units/ml.

The blood solution samples were then pooled and mixed with depyrogenated aqueous sodium citrate solution to form a 0.2% by weight solution of sodium citrate in bovine whole blood (hereafter "0.2% sodium citrate blood solution").

The 0.2% sodium citrate blood solution was then passed, in-series, through 800 µm and 50 µm polypropylene filters to remove large blood solution debris of a diameter approximately 50 µm or more.

The RBCs were then washed to separate extracellular plasma proteins, such as BSA or IgG, from the RBCs. To wash the RBCs contained in the blood solution, the volume of blood solution in the diafiltration tank was initially diluted by the addition of an equal volume of a filtered isotonic solution to diafiltration tank. The isotonic solution was filtered with a Millipore (Cat # CDUF 050 G1) 10,000 Dalton

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ultrafiltration membrane. The isotonic solution was composed of 6.0 g/l sodium citrate dihydrate and 8.0 g/l sodium chloride in water-for-injection (WFI).

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The diluted blood solution was then concentrated back to its original volume by diafiltration through a 0.2  $\mu$ m hollow fiber (Microgon Krosflo II microfiltration cartridge) diafilter. Concurrently, filtered isotonic solution was added continuously, as makeup, at a rate equal to the rate of filtrate loss through the 0.2  $\mu$ m diafilter.

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During diafiltration, components of the diluted blood solution which were significantly smaller in diameter than RBCs, or are fluids such as plasma, passed through the walls of the 0.2  $\mu$ m diafilter with the filtrate. RBCs, platelets and larger bodies of the diluted blood solution, such as white blood cells, were retained with continuously-added isotonic solution to form a dialyzed blood solution.

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During RBC washing, the diluted blood solution was maintained at a temperature between approximately 10 to 25°C with a fluid pressure at the inlet of the diafilter between about 25 psi and about 30 psi to improve process efficiency.

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RBC washing was complete when the volume of filtrate drained from the diafilter equaled about 600% of the volume of blood solution prior to diluting with filtered isotonic solution.

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The dialyzed blood solution was then continuously pumped at a rate of approximately 4 lpm to a Sharples Super Centrifuge, Model # AS-16, fitted with a #28 ringdam. The centrifuge was operating while concurrently being fed dialyzed blood solution, to separate the RBCs from the white blood cells and platelets.

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During operation, the centrifuge rotated at a rate sufficient to separate the RBCs into a heavy RBC phase, while also separating a substantial portion of the white blood cells (WBCs) and platelets into a light WBC phase, specifically about 15,000 rpm.

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A fraction of the RBC phase and of the WBC phase were separately and continuously discharged from the centrifuge during operation.

Following separation of the RBCs, the RBCs were lysed to form a hemoglobin-containing solution. A substantial portion of the RBCs were mechanically lysed while discharging the RBCs from the centrifuge. The cell membranes of the RBCs ruptured upon impacting the wall of RBC phase discharge line at an angle to the flow of RBC phase out of the centrifuge, thereby releasing hemoglobin (Hb) from the RBCs into the RBC phase.

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5 The lysed RBC phase then flowed through the RBC phase discharge line into  
a static mixer (Kenics ½ inch with 6 elements, Chemineer, Inc.). Concurrent with  
10 the transfer of the RBC phase to the static mixer, an equal amount of WFI was also  
injected into the static mixer, wherein the WFI mixed with the RBC phase. The  
5 flow rates of the RBC phase and the WFI into the static mixer are each at about 0.25  
lpm.

15 Mixing the RBC phase with WFI in the static mixer produced a lysed RBC  
colloid. The lysed RBC colloid was then transferred from the static mixer into a  
Sharples Super Centrifuge (Model # AS-16, Sharples Division of Alfa-Laval  
20 Separation, Inc.) which was suitable to separate the Hb from non-hemoglobin RBC  
components. The centrifuge was rotated at a rate sufficient to separate the lysed  
RBC colloid into a light Hb phase and a heavy phase. The light phase was  
composed of Hb and also contained non-hemoglobin components with a density  
25 approximately equal to or less than the density of Hb.

15 The Hb phase was continuously discharged from the centrifuge, through a  
0.45 µm Millipore Pellicon Cassette, Cat # HVLP 000 C5 microfilter, and into a  
holding tank in preparation for Hb purification. Cell stroma were then returned with  
30 the retentate from the microfilter to the holding tank. During microfiltration, the  
temperature within the holding tank was maintained at 10°C or less. To improve  
20 efficiency, when the fluid pressure at the microfilter inlet increased from an initial  
pressure of about 10 psi to about 25 psi, microfiltration was complete. The Hb  
35 microfiltrate was then transferred from the microfilter into the microfiltrate tank.

Subsequently, the Hb microfiltrate was pumped through a 100,000 Millipore  
Cat # CDUF 050 H1 ultrafilter. A substantial portion of the Hb and water,  
40 25 contained in the Hb microfiltrate, permeated the 100,000 Dalton ultrafilter to form a  
Hb ultrafiltrate, while larger cell debris, such as proteins with a molecular weight  
above about 100,000 Dalton, were retained and recirculated back into the  
microfiltrate tank. Concurrently, WFI was continuously added to the microfiltrate  
45 tank as makeup for water lost in the ultrafiltrate. Generally, cell debris include all  
30 whole and fragmented cellular components with the exception of Hb, smaller cell  
proteins, electrolytes, coenzymes and organic metabolic intermediates.  
Ultrafiltration continued until the concentration of Hb in the microfiltrate tank was

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less than 8 grams/liter (g/l). While ultrafiltering the Hb, the internal temperature of the microfiltrate tank was maintained at about 10°C.

The Hb ultrafiltrate was transferred into an ultrafiltrate tank, wherein the Hb ultrafiltrate was then recirculated through a 30,000 Dalton Millipore Cat # CDUF 050 T1 ultrafilter to remove smaller cell components, such as electrolytes, coenzymes, metabolic intermediates and proteins less than about 30,000 Daltons in molecular weight, and water from the Hb ultrafiltrate, thereby forming a concentrated Hb solution containing about 100 g Hb/L.

The concentrated Hb solution was then directed from the ultrafiltrate tank onto the media contained in parallel chromatographic columns (2 feet long with an 8 inch inner diameter) to separate the Hb by high performance liquid chromatography. The chromatographic columns contained an anion exchange medium suitable to separate Hb from nonhemoglobin proteins. The anion exchange media was formed from silica gel. The silica gel was exposed to  $\gamma$ -glycidoxypropylsilane to form active epoxide groups and then exposed to  $C_3H_7(CH_3)NCl$  to form a quaternary ammonium anion exchange medium. This method of treating silica gel is described in the *Journal of Chromatography*, 120:321-333 (1976).

Each column was pre-treated by flushing the chromatographic columns with a first buffer which facilitated Hb binding. Then 4.52 liters of the concentrated Hb solution were injected into each chromatographic column. After injecting the concentrated Hb solution, the chromatographic columns were then washed by successively directing three different buffers through the chromatographic columns to produce a Hb eluate, by producing a pH gradient within the columns. The temperature of each buffer during use was about 12.4°C. The buffers were prefiltered through a 10,000 Dalton ultrafiltration membrane before injection onto the chromatographic columns.

The first buffer, 20 mM tris-hydroxymethyl aminomethane (Tris) (pH about 8.4 to about 9.4), transported the concentrated Hb solution into the media in the chromatographic columns to bind the Hb. The second buffer, a mixture of the first buffer and a third buffer, with the second buffer having a pH of about 8.3, then adjusted the pH within chromatographic columns to elute contaminating non-hemoglobin components from the chromatographic columns, while retaining the Hb. Equilibration with the second buffer continued for about 30 minutes at a flow rate of

5 approximately 3.56 lpm per column. The elute from the second buffer was  
discarded to waste. The third buffer, 50 mM Tris (pH about 6.5 to about 7.5), then  
10 eluted the Hb from the chromatographic columns.

The Hb eluate was then directed through a sterile 0.22  $\mu$  Sartobran Cat #  
5 5232507 G1PH filter to a tank wherein the Hb eluate was collected. The first 3-to-  
4% of the Hb eluate and the last 3-to-4% of the Hb eluate were directed to waste.

15 The Hb eluate was further used if the eluate contained less than 0.05 EU/ml  
of endotoxin and contained less than 3.3 nmoles/ml phospholipids. To sixty liters of  
ultrapure eluate, which had a concentration of 100 g Hb/l, was added 9 l of 1.0 M  
20 NaCl, 20 mM Tris (pH 8.9) buffer, thereby forming a Hb solution with an ionic  
strength of 160 mM, to reduce the oxygen affinity of the Hb in the Hb solution. The  
Hb solution was then concentrated at 10°C, by recirculating through the ultrafilter,  
specifically a 10,000 Dalton Millipore Helicon, Cat # CDUF050G1 filter, until the  
25 Hb concentration was 110 g/l.

15 The Hb solution was then deoxygenated, until the  $pO_2$  of the Hb solution was  
reduced to the level where  $HbO_2$  content was about 10%, by recirculating the Hb  
solution at 12 lpm, through a 0.05  $\mu$ m Hoechst-Celanese Corporation Cat # G-  
30 240/40) polypropylene microfilter phase transfer membrane, to form a deoxygenated  
Hb solution (hereinafter "deoxy-Hb"). Concurrently, a 60 lpm flow of nitrogen gas  
20 was directed through the counter side of the phase transfer membrane. During  
deoxygenation, the temperature of the Hb solution was maintained between about 19  
35 °C and about 31°C.

Also during deoxygenation, and subsequently throughout the process, the Hb  
was maintained in a low oxygen environment to minimize oxygen absorption by the  
40 Hb and to maintain an oxygenated Hb (oxyhemoglobin or  $HbO_2$ ) content of less than  
25 about 10% in the deoxy-Hb.

The deoxy-Hb, 60 liters) was then diafiltered through an ultrafilter with 180 l  
of a storage buffer, containing 0.2 wt % N-acetyl cysteine, 33 mM sodium  
45 phosphate buffer (pH 7.8) having a  $pO_2$  of less than 50 torr, to form an oxidation-  
stabilized deoxy-Hb. Prior to mixing with the deoxy-Hb, the storage buffer was  
30 depyrogenated with a 10,000 Dalton Millipore Helicon, Cat # CDUF050G1  
depyrogenating filter.

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The storage buffer was continuously added at a rate approximately equivalent to the fluid loss across the ultrafilter. Diafiltration continued until the volume of fluid lost through diafiltration across the ultrafilter was about three times the initial volume of the deoxy-Hb.

5 Prior to transferring the oxidation-stabilized deoxy-Hb into a polymerization apparatus, oxygen-depleted WFI was added to the polymerization reactor to purge the polymerization apparatus of oxygen to prevent oxygenation of oxidation-stabilized deoxy-Hb. The amount of WFI added to the polymerization apparatus was that amount which would result in a Hb solution with a concentration of about 10 40 g Hb/l, when the oxidation-stabilized deoxy-Hb was added to the polymerization reactor. The WFI was then recirculated throughout the polymerization apparatus, to deoxygenate the WFI by flow through a 0.05  $\mu$ m polypropylene microfilter phase transfer membrane (Hoechst-Celanese Corporation Cat # 5PCM-108, 80 sq. ft.) against a counterflow of pressurized nitrogen. The flow rates of WFI and nitrogen 15 gas, through the phase transfer membrane, were about 18 to 20 lpm and 40 to 60 lpm, respectively.

After the  $pO_2$  of the WFI in the polymerization apparatus was reduced to less than about 2 torr  $pO_2$ , the polymerization reactor was blanketed with nitrogen by a flow of about 20 lpm of nitrogen into the head space of the polymerization reactor. 20 The oxidation-stabilized deoxy-Hb was then transferred into the polymerization reactor.

The polymerization was conducted in a 12 mM phosphate buffer with a pH of 7.8, having a chloride concentration less than or equal to about 35 mmolar.

25 The oxidation-stabilized deoxy-Hb and N-acetyl cysteine were subsequently slowly mixed with the cross-linking agent glutaraldehyde, specifically 29.4 grams of glutaraldehyde for each kilogram of Hb over a five hour period, while heating at 40°C and recirculating the Hb solution through a Kenics 1-1/2 inch static mixer with 6 elements (Chemineer, Inc.), to form a polymerized Hb (poly(Hb)) solution.

45 Recirculating the oxidation-stabilized deoxy-Hb and the glutaraldehyde through the static mixer caused turbulent flow conditions with generally uniform mixing of the glutaraldehyde with the oxidation-stabilized deoxy-Hb, thereby reducing the potential for forming pockets of deoxy-Hb containing high 50 concentrations of glutaraldehyde. Generally uniform mixing of glutaraldehyde and

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deoxy-Hb reduced the formation of high molecular weight poly(Hb) (having a molecular weight above 500,000 Daltons) and also permitted faster mixing of glutaraldehyde and deoxy-Hb during polymerization.

5 In addition, significant Hb intramolecular cross-linking resulted during Hb polymerization as an effect of the presence of N-acetyl cysteine upon the polymerization of Hb.

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After polymerization, the temperature of the poly(Hb) solution in the polymerization reactor was reduced to a temperature between about 15°C to about 25°C.

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10 The poly(Hb) solution was then concentrated by recirculating the poly(Hb) solution through the ultrafilter until the concentration of the poly(Hb) was increased to about 85 g/l. A suitable ultrafilter is a 30,000 Dalton filter (e.g., Millipore Helicon, Cat # CDUF050LT).

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15 Subsequently, the poly(Hb) solution was then mixed with 66.75 g sodium borohydride and again recirculated through the static mixer. Specifically, for every nine liters of poly(Hb) solution, one liter of 0.25 M sodium borohydride solution was added at a rate of 0.1 to 0.12 lpm.

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Prior to adding the sodium borohydride to the poly(Hb) solution, the pH of the poly(Hb) solution was basified by adjusting pH to a pH of about 10 to preserve the sodium borohydride and to prevent hydrogen gas formation. The pH of the poly(Hb) solution was adjusted by diafiltering the poly(Hb) solution with approximately 215 l of depyrogenated, deoxygenated 12 mM sodium borate buffer, having a pH of about 10.4 to about 10.6. The poly(Hb) solution was diafiltered by recirculating the poly(Hb) solution from the polymerization reactor through the 30 kD ultrafilter. The sodium borate buffer was added to the poly(Hb) solution at a rate approximately equivalent to the rate of fluid loss across the ultrafilter from diafiltration. Diafiltration continued until the volume of fluid lost across the ultrafilter from diafiltration was about three times the initial volume of the poly(Hb) solution in the polymerization reactor.

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30 Following pH adjustment, sodium borohydride solution was added to the polymerization reactor to reduce bonds in the poly(Hb) solution to bonds and to form stable poly(Hb) in solution. During the sodium borohydride addition, the poly(Hb) solution in the polymerization reactor was continuously recirculated

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through the static mixer and the 0.05  $\mu\text{m}$  polypropylene microfilter phase transfer membrane to remove dissolved oxygen and hydrogen. Flow through a static mixer also provided turbulent sodium borohydride flow conditions that rapidly and effectively mixed sodium borohydride with the poly(Hb) solution. The flow rates of poly(Hb) solution and nitrogen gas through the 0.05  $\mu\text{m}$  phase transfer membrane were between about 2.0 to 4.0 lpm and about 12 to 18 lpm, respectively. After completion of the sodium borohydride addition, reduction continued in the polymerization reactor while an agitator contained therein rotated at approximately 75 rotations per minute.

Approximately one hour after the sodium borohydride addition, the stable poly(Hb) solution was recirculated from the polymerization reactor through the 30,000 Dalton ultrafilter until the stable poly(Hb) solution concentration was 110 g/l. Following concentration, the pH and electrolytes of the stable poly(Hb) solution were restored to physiologic levels to form a stable polymerized Hb blood substitute, by diafiltering the stable poly(Hb) solution, through the 30,000 Dalton ultrafilter, with a filtered, deoxygenated, low pH buffer containing 27 mM sodium lactate, 12 mM NAC, 115 mM NaCl, 4 mM KCl, and 1.36 mM  $\text{CaCl}_2$  in WFI, (pH 5.0). Diafiltration continued until the volume of fluid lost through diafiltration across the ultrafilter was about 6 times the pre-diafiltration volume of the concentrated Hb product.

After the pH and electrolytes were restored to physiologic levels, the stable polymerized Hb blood substitute was then diluted to a concentration of 5.0 g/dl by adding the filtered, deoxygenated low pH buffer to the polymerization reactor. The diluted blood substitute was then diafiltered by recirculating from the polymerization reactor through the static mixer and a 100,000 Dalton purification filter against a filtered deoxygenated buffer containing 27 mM sodium lactate, 12 mM NAC, 115 mM NaCl, 4 mM KCl, and 1.36 mM  $\text{CaCl}_2$  in WFI, (pH 7.8). Diafiltration continued until the blood substitute contained less than or equal to about 10% modified tetrameric and unmodified tetrameric species by GPC when run under dissociating conditions.

The purification filter was run under conditions of low transmembrane pressure with a restricted permeate line. Following removal of substantial amounts of modified tetrameric Hb and unmodified tetrameric Hb, recirculation of the blood

substitute continued through the 30,000 Dalton ultrafilter until the concentration of the blood substitute was about 130 g/l.

The stable blood substitute was then stored in a suitable container having a low oxygen environment and a low oxygen in-leakage.

### Example 3

#### Hemoglobin Blood substitute Storage: Primary Package

The hemoglobin blood substitute, as prepared in Example 1 was packaged in an oxygen barrier primary package (E-13135 and E13242, American National Can). The construction of the primary package is discussed in detail above. The primary package is a laminate material having a thickness of about 0.005 in. (or about 127  $\mu\text{m}$ ), comprising a medium density polyethylene/ethylene vinyl alcohol layer, a nylon layer, and a linear low density polyethylene sealant layer. The oxygen permeability of the laminate is 0.0084 cc/100 in<sup>2</sup>/atm-day (25°C, 100%/50% RH) or  $1.3 \times 10^{-3}$  cc/cm<sup>2</sup>/atm-day (25°C, 100%/50%RH). The water vapor permeability is 25.0 mg/100 in<sup>2</sup>/atm-day (25°C, 100%/ 50% RH) (or 3.87 mg/100cm<sup>2</sup>/atm-day (25°C, 100%/50% RH)).

The packaged blood substitutes were maintained without overwrap under accelerated stability conditions for 90 days followed by sampling of the concentration and/or levels of N-acetyl-L-cysteine (NAC), bis-N-acetyl-L-cysteine (NAC<sub>2</sub>), total Hb (THb), oxygenated hemoglobin (HbO<sub>2</sub>) and methemoglobin (metHb). Accelerated stability conditions are 40°C and 75% relative humidity (RH). Because the barrier properties of the packaging material decrease at higher temperature and relative humidity, these accelerated stability conditions are comparable to stability measured under ambient conditions (25°C and 50% RH) for at least one year. The results are set forth in Table II.

Table II  
Accelerated Stability Data

Month	NAC (%)	NAC <sub>2</sub> (%)	THb (g/dl)	HbO <sub>2</sub> (%)	metHB (%)
0	0.18	0.01	12.4	3	1
3	0.03	0.21	12.0	3	6
Specification	≤0.24	≤0.24	12.0-14.0	≤10	≤15

#### Example 4

##### Polymerized Hemoglobin Analysis

The endotoxin concentration in the hemoglobin product is determined by the method "Kinetic/ Turbidimetric LAL 5000 Methodology" developed by Associates of Cape Cod, Woods Hole, Massachusetts, J. Levin *et al.*, *J. Lab. Clin. Med.*, 75:903-911 (1970). Various methods were used to test for any traces of stroma for example, a precipitation assay, immunoblotting, and enzyme-linked immunosorbent assay (ELISA) for a specific cell membrane protein or glycolipid known by those skilled in the art.

Particulate counting was determined by the method "Particulate Matter in Injections: Large Volume Injections for Single Dose Infusions", *U.S Pharmacopeia*, 22:1596, 1990.

To determine glutaraldehyde concentration, a 400 µl representative sample of the hemoglobin product was derivitized with dinitrophenylhydrazine and then a 100 µl aliquot of the derivative solution was injected onto a YMC AQ-303 ODS column at 27 °C, at a rate of 1 ml/min., along with a gradient. The gradient consisted of two mobile phases, 0.1% trifluoroacetic acid (TFA) in water and 0.08% TFA in acetonitrile. The gradient flow consisted of a constant 60% 0.08% TFA in acetonitrile for 6.0 minutes, a linear gradient to 85% 0.08% TFA in acetonitrile over 12 minutes, a linear gradient to 100% 0.08% TFA in acetonitrile over 4 minutes hold at 100% 0.08% TFA in acetonitrile for 2 minutes and re-equilibrate at 45% of 0.1% TFA in water. Ultraviolet detection was measured at @360 nm.

To determine NAC concentration, an aliquot of hemoglobin product was diluted 1:100 with degassed sodium phosphate in water and 50 µl was injected onto

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a YMC AQ-303 ODS column with a gradient. The gradient buffers consisted of a sodium phosphate in water solution and a mixture of 80% acetonitrile in water with 0.05% TFA. The gradient flow consisted of 100% sodium phosphate in water for 15 minutes, then a linear gradient to 100% mixture of 80% acetonitrile and 0.05% TFA over 5 minutes, with a hold for 5 minutes. The system was then re-equilibrated at 100% sodium phosphate for 20 minutes.

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Phospholipid analysis was done by a method based on procedures contained in the following two papers: Kolarovic *et al.*, "A Comparison of Extraction Methods for the Isolation of Phospholipids from Biological Sources", *Anal. Biochem.*, 156:244-250, 1986 and Duck-Chong, C. G., "A Rapid Sensitive Method for Determining Phospholipid Phosphorus Involving Digestion With Magnesium Nitrate", *Lipids*, 14:492-497, 1979.

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Osmolarity was determined by analysis on an Advanced Cryomatic Osmometer, Model #3C2, Advanced Instruments, Inc., Needham, Massachusetts.

Total hemoglobin, methemoglobin and oxyhemoglobin concentrations were determined on a Co-Oximeter Model #482, from Instrumentation Laboratory, Lexington, Massachusetts.

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Na<sup>+</sup>, K<sup>+</sup>, Cl<sup>-</sup>, Ca<sup>++</sup>, pO<sub>2</sub> concentrations were determined by a Novastat Profile 4, Nova Biomedical Corporation, Waltham, Massachusetts.

Oxygen binding constant, P<sub>50</sub> was determined by a Hemox-Analyzer, TCS Corporation, Southampton, Pennsylvania.

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Temperature and pH were determined by standard methods known by those skilled in the art.

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Molecular weight (M.W.) was determined by conducting gel permeation chromatography (GPC) on the hemoglobin products under dissociating conditions. A representative sample of the hemoglobin product was analyzed for molecular weight distribution. The hemoglobin product was diluted to 4 mg/ml within a mobile phase of 50 mM Bis-Tris (pH 6.5), 750 mM MgCl<sub>2</sub>, and 0.1 mM EDTA. This buffer serves to dissociate Hb tetramer into dimers, that have not been cross-linked to other Hb dimers through intramolecular or intermolecular crosslinks, from the poly(Hb). The diluted sample was injected onto a TosohHaas G3000SW column. Flow rate was 0.5 ml/min. and ultraviolet detection was recorded at 280 nm.

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The results of the above tests on veterinary (OXYGLOBIN™) and human Hb blood substitutes, formed according to the method of invention, are summarized in Tables III and IV, respectively.

Table III

PARAMETER	RESULTS
pH (18-22°C)	physiologically acceptable pH
Endotoxin	< 0.5 EU/ml
Sterility Test	Meets Test
Phospholipids <sup>a</sup>	<3.3 nm/ml
Total Hemoglobin	12.0 - 14.0 g/dl
Methemoglobin	<15%
Oxyhemoglobin	<10%
Sodium, Na <sup>+</sup>	145-160 mM
Potassium, K <sup>+</sup>	3.5-5.5 mM
Chloride, Cl <sup>-</sup>	105-120 mM
Calcium, Ca <sup>++</sup>	0.5-1.5 mM
Boron	<10 ppm
Osmolality	290-310 mOsm
Glutaraldehyde	<3.5 µg/ml
N-acetyl-L-cysteine	<0.2%
M.W. >500,000	<15%
Unmodified Tetramer	<5%
Particulate Content >10µ	<12/ml
Particulate Content >25µ	<2/ml

<sup>a</sup>-measured in Hb before polymerization

Table IV

PARAMETER	RESULTS
pH (18-22°C)	Physiologically acceptable pH
Endotoxin	< 0.5 EU/ml
Sterility Test	Meets Test
Phospholipids <sup>a</sup>	<3.3 nm/ml
Total Hemoglobin	12.0 - 14.0 g/dl
Methemoglobin	<15%
Oxyhemoglobin	<10%
Sodium, Na <sup>+</sup>	145-160 mM
Potassium, K <sup>+</sup>	3.5-5.5 mM
Chloride, Cl <sup>-</sup>	105-120 mM
Calcium, Ca <sup>++</sup>	0.5-1.5 mM
Boron	<10 ppm
Osmolality	290-310 mOsm
Glutaraldehyde	<3.5 µg/ml
N-acetyl-L-cysteine	≤0.2%
M.W. >500,000	≤15%
M.W. ≤ 65,000	<10%
M.W. <32,000	<5%
Particulate Content >10µ	<12/ml
Particulate Content >25µ	<2/ml

<sup>a</sup>-measured in Hb before polymerization

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Those skilled in the art will recognize, or be able to ascertain using no more than routine experimentation, many equivalents to the specific embodiments of the invention described herein. These and all other such equivalents are intended to be encompassed by the following claims.

**Claims**

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## CLAIMS

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The invention claimed is:

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1. A method for preserving a deoxygenated hemoglobin blood substitute comprising maintaining the deoxygenated hemoglobin blood substitute in an oxygen barrier film primary package that includes a transparent polymer material having at least one layer, said primary package having an oxygen permeability of less than about 1.0 cc per 100 square inches per 24 hours per atmosphere at about 25°C and an external relative humidity of about 50%.
2. The method of Claim 1, wherein the transparent polymer material comprises an oxygen barrier layer.
3. The method of Claim 2, wherein the oxygen barrier layer comprises ethylene vinyl alcohol.
4. The method of Claim 2, wherein the polymer material comprises an outer layer that includes polyolefin.
5. The method of Claim 4, wherein said outer layer comprises medium density polyethylene.
6. The method of Claim 5, wherein the outer layer and the oxygen barrier layer are co-extruded.
7. The method of Claim 2, wherein the oxygen barrier layer comprises a silicon oxide coated polyester layer.
8. The method of Claim 1, wherein the polymer material comprises an inner layer comprising polyolefin.

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9. The method of Claim 8, wherein the inner layer comprises linear low density polyethylene.
10. The method of Claim 1 wherein the hemoglobin blood substitute is maintained under a nitrogen, argon or helium atmosphere.
11. A preserved deoxygenated hemoglobin blood substitute, comprising:
  - a) a deoxygenated hemoglobin blood substitute; and
  - b) an oxygen barrier film primary package that includes a transparent polymer material having at least one layer, said primary package having an oxygen permeability of less than about 1.0 cc per 100 square inches per 24 hours per atmosphere at about 25°C and an external relative humidity of about 50%, within which the deoxygenated hemoglobin blood substitute is sealed, thereby preserving the deoxygenated hemoglobin blood substitute in an environment that is substantially free of oxygen.
12. The preserved deoxygenated blood substitute of Claim 11, wherein the transparent polymer material includes an oxygen barrier layer.
13. The preserved deoxygenated blood substitute of Claim 12, wherein the oxygen barrier layer comprises ethylene vinyl alcohol.
14. The preserved deoxygenated blood substitute of Claim 12, wherein the polymer material comprises an outer layer that includes polyolefin.
15. The preserved deoxygenated blood substitute of Claim 14, wherein said outer layer comprises medium density polyethylene.
16. The preserved deoxygenated blood substitute of Claim 15 wherein the medium density layer and the oxygen barrier layer are co-extruded.

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17. The preserved deoxygenated blood substitute of Claim 11, wherein the oxygen barrier layer comprises a silicon oxide coated polyester layer.

18. The preserved deoxygenated blood substitute of Claim 11, wherein the polymer material comprises an inner layer comprising polyolefin.

19. The preserved deoxygenated blood substitute of Claim 18, wherein the inner layer comprises linear low density polyethylene.

20. The preserved deoxygenated blood substitute of Claim 11, wherein the hemoglobin blood substitute is maintained under a nitrogen, argon or helium atmosphere.

## INTERNATIONAL SEARCH REPORT

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PCT/US 99/23631A. CLASSIFICATION OF SUBJECT MATTER  
IPC 7 A01N1/02 A01J1/00

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

IPC 7 A01N A01J

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practical, search terms used)

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category *	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X	US 5 691 452 A (GAWRYL MARIA S ET AL) 25 November 1997 (1997-11-25) cited in the application claims column 2, line 50 -column 3, line 58 column 19; example 2	1-20

☐ Further documents are listed in the continuation of box C.☒ Patent family members are listed in annex.

## \* Special categories of cited documents:

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# INTERNATIONAL SEARCH REPORT

Information on patent family members

Int. Patent Application No.

PCT/US 99/23631

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